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Wollin

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(54) **APPARATUS AND METHOD FOR MAGNETIC RESONANCE MEASUREMENT AND MAPPING OF ELECTRICAL IMPEDANCE, COMPLEX PERMITTIVITY AND COMPLEX CONDUCTIVITY AS APPLIED TO DETECTION AND EVALUATION OF SAMPLE PATHOLOGY**

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(51) **Int. Cl.**
A61B 5/05 (2006.01)

(52) **U.S. Cl.** **600/407**

(58) **Field of Classification Search** 600/407,
600/410-411, 415, 421-422, 425, 427, 547;
324/307, 309

See application file for complete search history.

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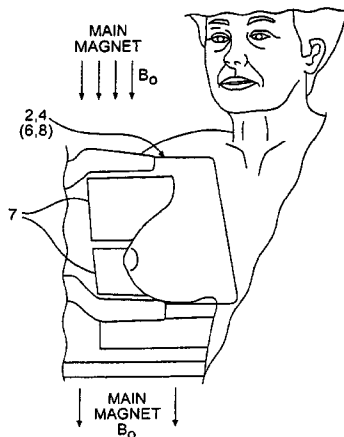
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(57) **ABSTRACT**

A method of measurement of or mapping the distribution of complex permittivity, complex conductivity, complex impedance, or electric loss angle during magnetic resonance imaging or analysis. The method includes applying a time-varying electric field of a Faraday shield to a sample and cross-correlating the line spectrum signal so produced with the voltage applied to the Faraday shield in a detection circuit. The method permits non-contrast magnetic resonance screening for breast cancer in vivo and/or continuous measurement of electrical characteristics of materials at variable frequencies in vitro. A system of detecting and evaluating sample pathology includes a Faraday shield device that includes parallel electrodes oriented orthogonal to the static magnetic field of a MRI device to produce a time varying electric field. A detector is coupled to the MRI device to detect at least one of a complex permittivity, a complex conductivity, and an electrical impedance of the sample.

36 Claims, 6 Drawing Sheets



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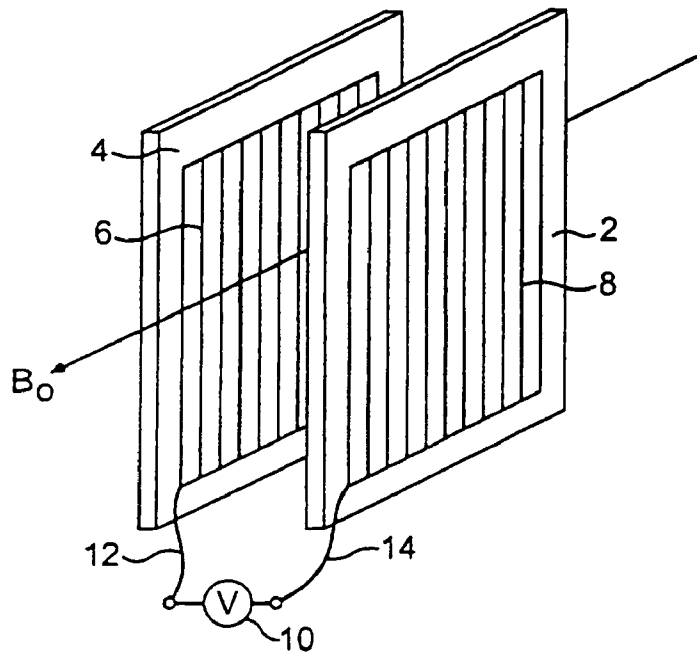


FIG. 1

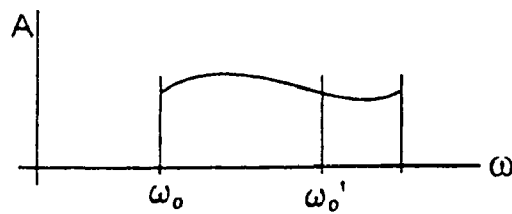


FIG. 3

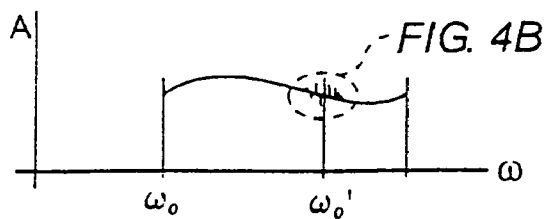
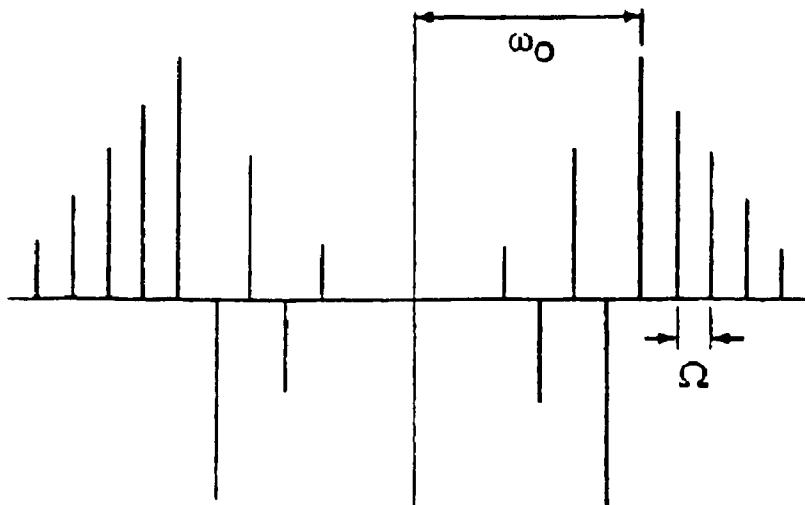


FIG. 4A



FIG. 4B

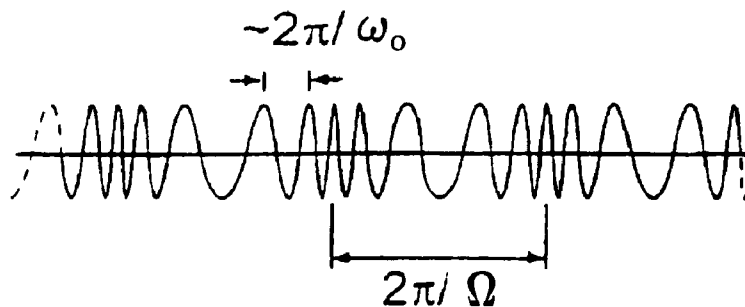
FREQUENCY DOMAIN



$$\pi \sum_{n=-\infty}^{+\infty} \left[J_n \left(\frac{\gamma b}{\Omega} \right) \delta(\omega - \omega_0 - n\Omega) + J_n \left(\frac{\gamma b}{\Omega} \right) \delta(\omega + \omega_0 + n\Omega) \right]$$

FIG. 2A

TIME DOMAIN



$$\cos \left(\frac{\gamma b}{\Omega} \sin \Omega t + \omega_0 t \right)$$

FIG. 2B

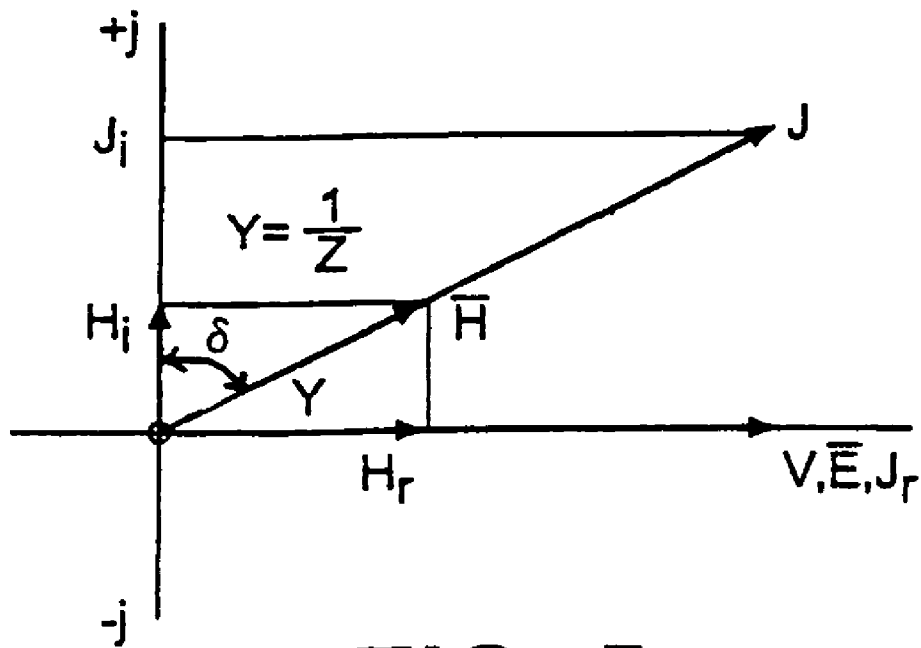


FIG. 5

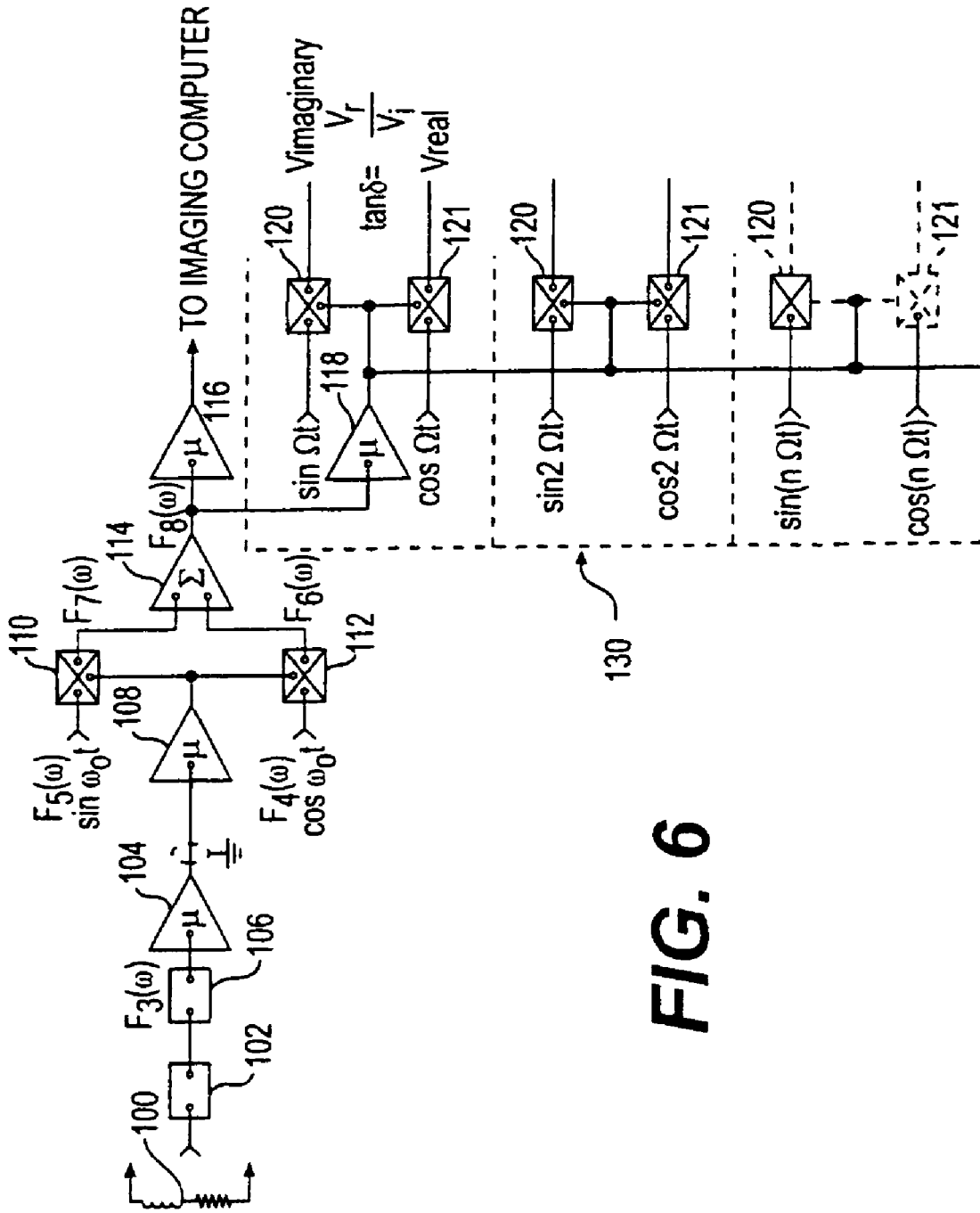


FIG. 6

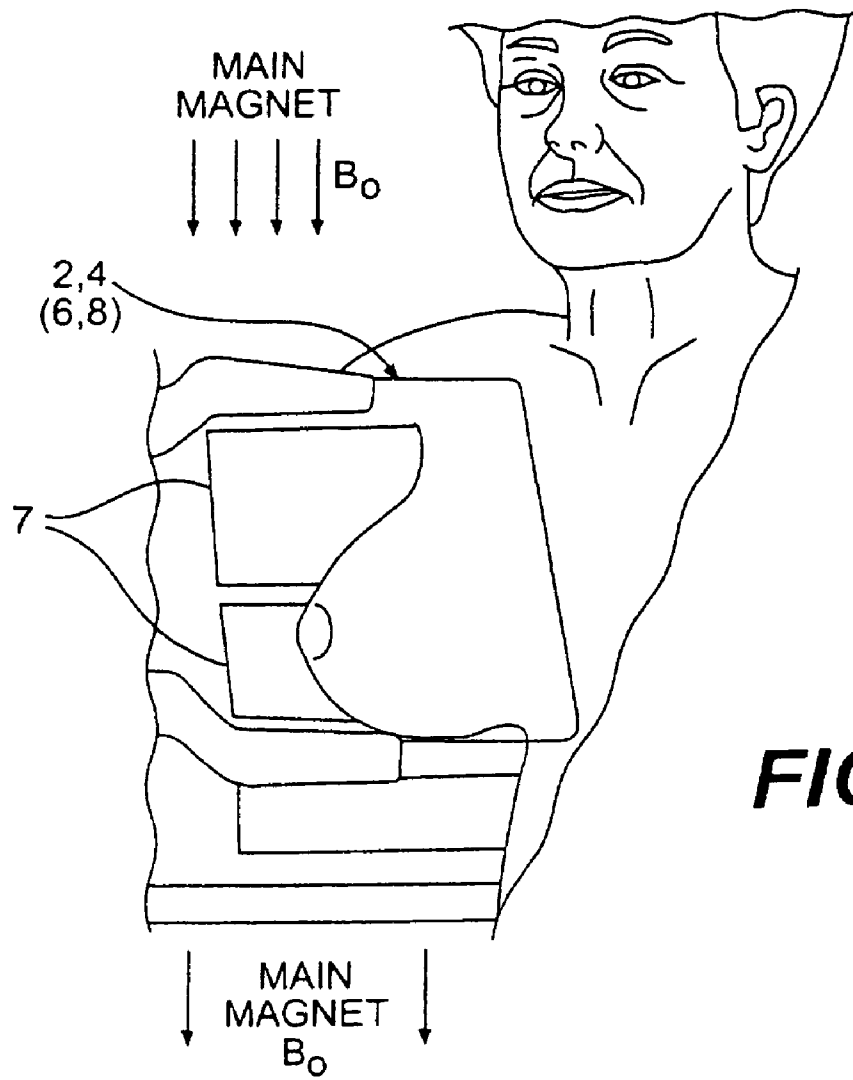


FIG. 7

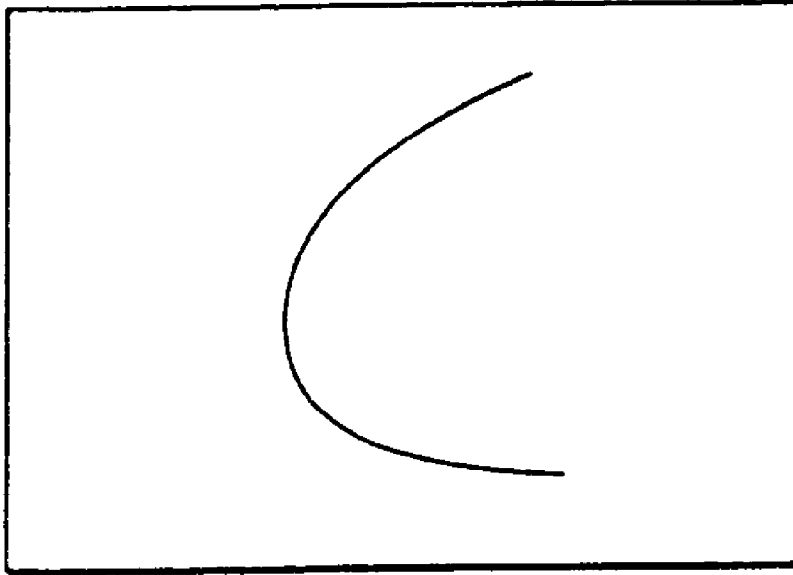


FIG. 8A

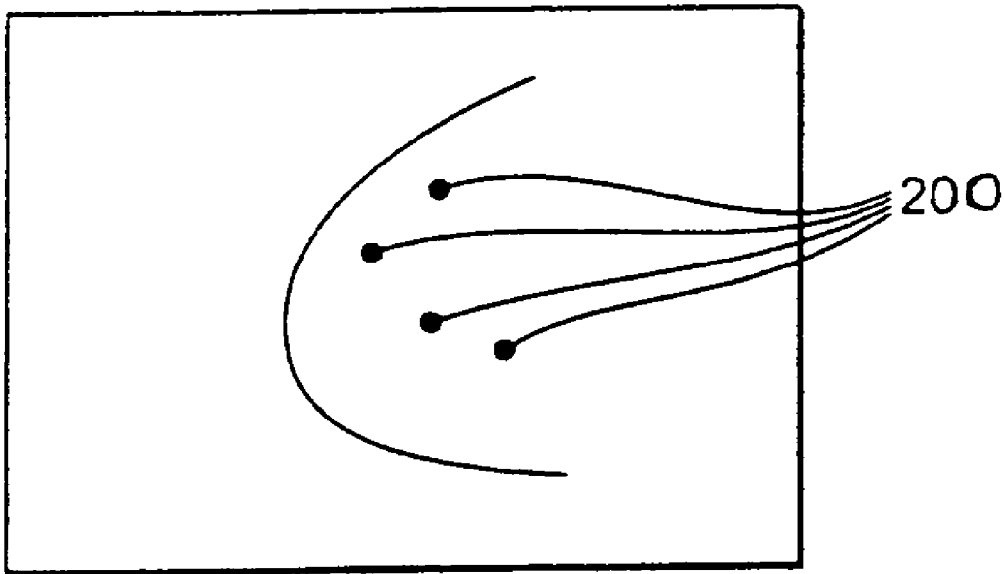


FIG. 8B

**APPARATUS AND METHOD FOR MAGNETIC
RESONANCE MEASUREMENT AND
MAPPING OF ELECTRICAL IMPEDANCE,
COMPLEX PERMITTIVITY AND COMPLEX
CONDUCTIVITY AS APPLIED TO
DETECTION AND EVALUATION OF SAMPLE
PATHOLOGY**

RELATED APPLICATIONS

This application claims benefit of priority to PCT Application No. PCT/US03/27122, filed on Aug. 29, 2003 and Provisional Application No. 60/406,924, filed on Aug. 30, 2002, incorporated by reference herein in its entirety.

BACKGROUND OF THE INVENTION

This invention generally relates to magnetic resonance and more particularly to the measurement of electrical impedance, complex permittivity, and/or complex conductivity by the application of time-varying electric fields in an imaging volume (especially as it enables detection and evaluation of sample, e.g., human breast, pathology) or in a homogeneous sample volume (especially as it relates to industrial materials testing).

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SUMMARY OF THE INVENTION

The present invention provides a method for large population screening for breast cancer without the use of ionizing radiation or the parenteral administration of medications. It also provides a method for continuously measuring the dielectric properties of materials in a manufacturing process at variable frequencies.

An object of this invention is to provide a non-invasive, non-contrast, non-ionizing radiation imaging method for screening a sample for cancer by providing an attachment to existing magnetic resonance imaging ("MRI") machines. By non-contrast, it is meant that injection of a contrast agent (e.g., Gadolinium compounds) is not required (but still could be used). It is possible, however, to use a contrast agent. An additional object of this invention is to provide a method for measuring the electrical impedance, complex permittivity, and/or complex conductivity of a homogeneous sample in a materials testing or production control application by providing an attachment to existing magnetic resonance analysis machines.

According to one embodiment of the present invention, a method of detecting and evaluating spatially distributed sample pathology may include placing a sample to be measured in a magnetic resonance imaging device, providing a Faraday shield device having an electrode array, applying a potential distribution to the Faraday shield device which produces a time varying electric field \vec{E} in the sample, which creates a spatially distributed current field \vec{J} , which generates time varying focal periodic aberrations in the local magnetic field \vec{b}_0 that periodically vary the phase of spins within the sample, and measuring or mapping at least one of complex permittivity, complex conductivity, and electrical impedance of the sample. This embodiment is applicable to, e.g., spatially ordered anatomic and pathological analysis of sample pathology utilizing a conventional magnetic resonance imaging device with a detection circuit attachment. In another aspect, the method may further comprise measuring the complex permittivity at a phase modulating frequency of the time varying potential distribution.

According to another embodiment of the present invention, a method of detecting and evaluating sample spatially ordered pathology may comprise: placing a human breast to be measured in a Faraday shield device having electrodes; applying to the Faraday shield device a time varying potential having a phase modulating frequency, which creates a time varying electric field \vec{E} in the breast, which creates a time varying current field in the breast, which periodically varies a phase of spins within the breast; and measuring a complex permittivity distribution of the breast at the phase modulating frequency.

According to another embodiment of the present invention, a method of measuring dielectric properties by the application of time-varying electric fields in a sample may include placing the sample in a magnetic resonance device, providing a Faraday shield device, and applying a potential distribution V to the Faraday shield device, which generates a time varying electric field \vec{E} in the sample, which creates a time varying current field \vec{J} in the sample, which creates/generates a periodic magnetic field \vec{b}_0 that periodically varies the phase of spins within the sample, and measuring at least one of complex permittivity, complex conductivity, and electrical impedance of the sample with a detection circuit attachment. This embodiment is applicable to continuous measurement of dielectric properties at a controllable frequency Ω .

According to another embodiment of the present invention, a system of detecting and evaluating spatially distributed sample pathology may include a magnetic resonance imaging device to produce an image of a sample (the magnetic resonance imaging device generating a static magnetic field \vec{B}_0 and gradient fields \vec{G}), a radio frequency generator operating near the Larmor frequency ω_0 and including receiving coils

and transmitting coils or transmitter-receiver coils). The system further includes a Faraday shield that includes parallel electrodes oriented orthogonal to the static magnetic field to produce a time varying electric field in the sample. A voltage source may also be provided and adapted to apply a periodic voltage V at a frequency Ω to the Faraday shield device. A detector may also be provided to detect one of a complex permittivity, a complex conductivity, and an electrical impedance of the sample.

According to a preferred aspect of the present invention, the sample may be a human breast. The Faraday shield device may comprise a pair of compression paddles and the electrodes may be oriented in parallel to each other. The electrodes may be embedded in an insulating material. The insulating material may have a high dielectric constant and may comprise one or more ferroelectric materials. According to another preferred aspect of the present invention, the electrodes may be further oriented substantially perpendicular to the main magnetic field B_0 of the magnetic resonance imaging device.

According to another preferred aspect of the present invention, the Faraday shield device may comprise a pair of compression paddles, and the method may further comprise: placing the Faraday shield within an imaging region of the magnetic resonance imaging device; and placing one of the receiver coil and the transmitter-receiver coil of the magnetic resonance imaging device near the compression paddles.

According to another preferred aspect of the present invention, the method may further comprise detecting orthogonal components of each sideband of a line spectrum resolved with respect to the phase of a voltage applied to the Faraday shield device. The method may further comprise determining a ratio of the resolved real and imaginary components of the sidebands. The method may further comprise determining an electric loss angle of the sample. The method may further comprise detecting orthogonal components of each sideband of a line spectrum resolved with respect to the phase of a voltage applied to the Faraday shield device at a frequency $\Omega \ll$ (or much less than) ω_0 , the Larmor frequency of the magnetic resonance imaging device. The method may further comprise identifying focal aberrations contained in an image produced by the magnetic resonance imaging device.

According to another embodiment of the present invention, a method of measuring electrical impedance by the application of time-varying electric fields in an imaging volume may comprise: placing a sample in a magnetic resonance device; providing a detector to the magnetic resonance device; providing a Faraday shield device about the sample, where the Faraday shield device may include electrodes oriented parallel to each other; applying a periodic potential distribution across the Faraday shield device to create a time varying electric field in the sample, which creates a local time varying current field in the sample, wherein the local time varying current field creates a periodic aberration in a local magnetic field that periodically varies a phase of spins within the sample; and measuring an electrical impedance of the sample with the detector.

According to another embodiment of the present invention, a system of detecting and evaluating sample pathology may comprise: a magnetic resonance imaging device to produce an image of a sample, the magnetic resonance imaging device generating a static magnetic field and including one of receiving coils and transmitter-receiver coils; a Faraday shield device that includes parallel electrodes oriented orthogonal to the static magnetic field connected to a voltage source adapted to generate a periodic voltage V at a frequency Ω ; and

a detector to detect one of a complex permittivity, a complex conductivity, and an electrical impedance of the sample.

In a preferred aspect of the present invention, the detector may comprise: first demodulators supplied with a quadrature output at a Larmor frequency ω_0' from a magnetic resonance master radio frequency oscillator; a first amplifier to sum first output signals from the first demodulators; a second amplifier to receive a second output signal from the summing amplifier; and second demodulators coupled to the second amplifier to provide cross-correlated outputs corresponding to at least one of real and imaginary components that correspond to a signal received by the one of receiver and transmitter-receiver coils from a location x in the sample, and corresponding to the frequency ω_0' resolved with respect to a phase of V . The second demodulators may comprise a series n of double-balanced demodulator pairs, each double balanced demodulator pair coupled to the second amplifier, to provide cross-correlated outputs corresponding to real and/or imaginary components of the signal received by the one of receiver coils and transmitter-receiver coils from the location x in the sample. The second demodulators may be supplied with frequency sources $\sin(n\Omega t)$ and $\cos(n\Omega t)$.

In another preferred aspect of the present invention, the system may further comprise a processor to analyze the cross-correlated outputs of the second demodulators and to provide the complex permittivity at the location x at frequency Ω . The Faraday shield may include a pair of non-conductive compression paddles, each compression paddle comprising an electrode array contained in an insulating portion thereof and coupled to the voltage source. At least one of receiving coils and transmitter-receiver coils may be disposed near at least one of the compression paddles. In another preferred aspect of the present invention, the periodic voltage may be either continuously applied or pulsed.

According to another embodiment of the present invention, a system for measuring the electrical impedance of a sample may comprise: a magnetic resonance device; a Faraday shield device disposed about the sample, where the Faraday shield device may include a pair of electrode arrays oriented substantially parallel to each other and substantially orthogonal to the static magnetic field of the magnetic resonance device; a voltage source to apply a periodic potential distribution across the Faraday shield device to create a time varying electric field in the sample, which creates a local time varying current field in the sample, which creates a periodic aberration in a local magnetic field that periodically varies a phase of spins within the sample; and a detector coupled to the magnetic resonance device to measure a value corresponding to an electrical impedance of the sample.

Further features and advantages of the invention, as well as the structure and operation of various embodiments of the invention, are described in detail below with reference to the accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

The accompanying drawings, which are incorporated in, and form a part of, the specification, illustrate some embodiments of the present invention and, together with the description, serve to explain the principles of the invention. In the drawings:

FIG. 1 represents an exemplary embodiment of breast compression paddles, each containing a parallel array of electrodes forming a Faraday shield, with the electrodes oriented perpendicular to the main magnetic field \vec{B}_0 of the magnetic resonance (imaging) device.

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FIG. 2 represents the frequency spectrum of an isolated spin subjected to a time-varying magnetic field b of frequency Ω at position x corresponding to a Larmor frequency ω_o' in a magnetic resonance device.

FIG. 3 represents a band spectrum produced by a clinical magnetic resonance imaging machine during the "read" time, as is known in the art.

FIGS. 4A and 4B represent the superposition of FIG. 2 and FIG. 3 to produce a local aberration of signal distribution centered about frequency ω_o' which corresponds to the Larmor frequency at position x .

FIG. 5 represents the temporal phase relationships of the voltage \check{V} applied to the Faraday shield device, the electric field \check{E} , the local complex admittance \check{Y} or impedance \check{Z} of the breast or specimen, the local current flux density \check{J} produced by the electric field \check{E} , the temporal orthogonal components \check{J}_r and \check{J}_i of \check{J} , the temporal orthogonal components \check{H}_r and \check{H}_i of the local magnetic field intensity \check{H} produced by \check{J} , and the electric loss angle δ of the local complex admittance or impedance.

FIG. 6 represents an exemplary detector circuit 130 according to an embodiment of the invention that connects to the magnetic resonance (imaging) device for detection of the temporal orthogonal components of each sideband resolved with respect to the phase of the voltage V of frequency Ω applied to the Faraday shield device, the ratio of which sideband components yields $\tan \delta$, where δ is the electric loss angle.

FIG. 7 shows an illustration of a magnetic resonance (imaging) device incorporating the compression device according to an embodiment of the present invention.

FIG. 8A, shows a first image of a breast with the Faraday shield voltage V turned off and FIG. 8B shows an image of the same breast with the Faraday shield voltage V turned on.

DESCRIPTION OF THE EXEMPLARY EMBODIMENTS

According to the present invention, a non-invasive device and method is provided to permit the measurement an/or mapping of electrical impedance, complex permittivity and complex conductivity of a sample with distributed physical properties and/or the electrical impedance of a homogeneous sample. A magnetic resonance imaging ("MRI") device can be implemented to permit the measurement of electrical impedance, complex permittivity and complex conductivity of a sample, such as a human breast. In this embodiment, measurement can be made by the application of a potential distribution across a Faraday shield device implemented with the magnetic resonance imaging device which produces a time varying electric field \check{E} in the sample, which creates a spatially distributed current field \check{J} , which generates time varying focal periodic aberrations in the local magnetic field \check{b}_o that periodically vary the phase of spins within the sample. The device and method of this embodiment can thus provide the location of sample pathology for detection and both anatomic and pathological evaluation. In a homogeneous sample embodiment, a magnetic resonance device measurement can be made by the application of a potential distribution across a Faraday shield device implemented with the magnetic resonance imaging device which produces a time varying electric field in the sample, which creates a current field, which generates time varying periodic aberrations in the local magnetic field that periodically vary the phase of spins within the sample. A detection circuit is provided to yield an output that

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corresponds to the electrical impedance, complex permittivity and/or complex conductivity.

According to one embodiment of the present invention, the sample or object to be measured or mapped, for example a human breast, is placed within a Faraday shield device connected to a time-varying voltage source V of frequency Ω so as to produce a time varying electric field \check{E} about the Faraday shield device, where

$$\check{E} = -\nabla \check{V} \quad \text{Eq. 1}$$

through Poisson's equation (in the quasi-static state)

$$\nabla \cdot (\check{\epsilon} \nabla \check{V}) = \check{\rho} \quad \text{Eq. 2}$$

where $\check{\epsilon}$ is the complex permittivity and $\check{\rho}$ is the charge distribution. This time-varying electric field creates a current distribution \check{J} in the sample or object whose intensity and phase is related to the applied electric field through the spatial distribution of the complex permittivity, complex conductivity, or electrical impedance of the sample or object. The Faraday shield device is arranged so that the current distribution in the sample being tested or object being imaged is essentially orthogonal to the main magnetic static field (present as an essential component of all magnetic resonance imaging devices as is known in the art). The time varying current field in the sample or object creates a periodic magnetic field \check{b}_o superimposed on the main magnetic field \check{B}_o and the gradient fields \check{G} which periodically varies the phase of the spins within the sample or object, inducing a line-spectrum of sideband frequencies in a receiver coil of the MRI device centered at the Larmor frequencies of the spins of the sample or object, (as is known in the art, Larmor frequencies ω_o can be made to be a function of spin location by the application of gradient fields) which sidebands are spaced by integral multiples of the phase modulating frequency Ω . Each sideband amplitude and sideband temporal phase is functionally related to the known applied voltage distribution \check{V} through the complex permittivity, complex conductivity, or electric impedance distribution. The frequency at which the complex permittivity, complex conductivity, or electrical impedance distribution is mapped or measured is the frequency Ω of the periodic voltage distribution \check{V} applied to the Faraday shield device.

In an embodiment of the present invention, a breast screening application using a magnetic resonance device, a human breast is positioned in a compression device (e.g., such as that shown in FIG. 1, and described in further detail below). The MRI device can be a conventional MRI device, which provides magnetic resonance images of a sample. Example MRI devices are described in the inventor's prior U.S. Pat. Nos. 5,412,322 and 5,757,187, incorporated by reference herein in their entirety. Further, a local receiver coil or a transmitter-receiver coil (as is known in the art), can be applied directly on or near a surface of the compression device, as is further illustrated in FIG. 7. The coil should be near enough to the compression device that a signal from the tissue (e.g., breast tissue) within the compression device can be received, as known to one skilled in the art. With this configuration, or a similar variant based on the present teachings, a periodic voltage \check{V} be continuously applied to the Faraday shield device creating a current flux distribution \check{J} in the breast producing local periodic alterations \check{b}_o in the ambient magnetic field at breast pathology sites associated with focal aberrations in complex permittivity, complex conductivity, and/or electrical impedance.

The component of the image produced by the magnetic resonance imaging device during each individual "read"

period will contain spatially ordered focal aberrations marking the location of suspected pathology. According to an embodiment of the present invention, the temporal analysis of the signal received from these focal aberrations, resolved with respect to the phase of the applied voltage \check{V} produces an estimation of the relative permittivity, complex conductivity, and/or electrical impedance yielding information about the pathology present as a function of position x corresponding to the Larmor frequency ω_o . Thus, the nature, extent, and distribution of pathology can be better estimated for biopsy, medical or surgical treatment, or conservative management without the use of ionizing radiation and preferably without the injection of magnetic resonance contrast agents.

FIG. 1 illustrates a compression device which includes a pair of breast compression paddles **2, 4**. Incorporated on or in the paddles **2, 4** are electrode arrays **6, 8**, which electrodes form a Faraday shield. According to one embodiment of the present invention, the electrode arrays **6, 8** are embedded or placed within an insulating material. The insulating material preferably has a high dielectric constant and can be formed with one or more ferroelectric materials. According to an alternative embodiment of the present invention, the electrode arrays **6, 8** or electrically equivalent arrays are not required to be embedded or placed within insulating material, which enables the Faraday shield device **6, 8** to make electrical conductivity contact with the sample.

The parallel electrodes of the Faraday shield are oriented perpendicular to the main magnetic field \vec{B}_0 of the magnetic resonance (imaging) device. A purpose of the Faraday shield of the present invention is to apply a potential distribution \check{V} across the breast to be imaged or to the sample to be analyzed without significantly affecting the B_1 radio frequency field intrinsic to conventional magnetic resonance devices (as in known in the art). This purpose can be achieved by orienting the parallel electrodes of the Faraday shield perpendicular to the main magnetic field B_0 so as not to provide a conduction path either for the electric field associated with the B_1 radio frequency field or additionally for eddy currents resulting from the application of gradients \vec{G} (intrinsic in all magnetic resonance imaging devices, as is known in the art). The electrode arrays are connected to a time varying voltage source (V) **10** of frequency Ω via connections **12** or **14** so as to produce a time varying electric field \vec{E} in the object. The voltage (\check{V}) can be applied continuously during the imaging sequence. Alternatively, the voltage (\check{V}) can be switched on only during the "read" period. Alternatively, the voltage (\check{V}) can be synchronized with the event sequence of the MRI device.

Applying a potential distribution \check{V} across the Faraday shield device creates a time varying electric field \vec{E} in the sample, which creates a current distribution \check{J} in the sample or object whose local intensity and phase is related to the applied electric field through the spatial distribution of the complex permittivity, complex conductivity, or electrical impedance of the sample or object. The frequency Ω of the periodic voltage V is related to the Larmor frequency ω_o as follows: $\Omega \ll \omega_o$. Example frequency values would be apparent to one of ordinary skill in the art given the present teachings.

As an example implementation, FIG. 7 illustrates the compression of the breast by the compression paddles **2, 4** which incorporate electrodes arrays **6, 8** and a preferred position of a conventional local receiver coil or transmitter-receiver coil **7**, which is preferably placed directly on or near a free surface of compression paddles **2** or **4** (as known in the art) within a conventional MRI device or system.

Using the paddles as illustrated, the current distribution \check{J} in the sample or object is essentially orthogonal to the main magnetic static field. The local time varying current field in the sample or object creates a periodic aberration in the local magnetic field, which periodically varies the phase of the spins within the sample or object, producing a line-spectrum of frequencies (see e.g., FIG. 2) in the receiver coil of the magnetic resonance (imaging) device spaced by integral multiples of the phase modulating frequency Ω about a central r.f. (Larmor) frequency ω_o corresponding to a position x .

In particular, a detector according to an embodiment of the present invention can be used to resolve the complex permittivity, complex conductivity, and/or electrical impedance detected in the sample. An example detector/detection circuit is shown in FIG. 6. The detector measures the complex permittivity at an image location x corresponding to frequency ω_o' during the "read" portion of the acquisition sequence. Synchronous demodulators **110** and **112** can be supplied with frequency sources **F4** and **F5** in quadrature at frequency ω_o' and synchronous detectors **120** can be supplied with frequency sources $\sin(n\Omega t)$ and $\cos(n\Omega t)$, where Ω is the frequency of the voltage \check{V} applied to the compression paddles or electrodes. The frequency at which the complex permittivity, complex conductivity, and/or electrical impedance distribution is mapped or measured is the frequency Ω of the periodic spatially ordered voltage distribution applied to the Faraday shield device and can be variable to make measurements as a function of frequency. This detector is described in further detail below.

FIG. 2 represents the frequency spectrum of an isolated spin subjected to a time-varying magnetic field such as would be created at each position x corresponding to the Larmor frequency ω_o' by the time-varying magnetic field produced by the distributed current density J ,

$$\text{where } \omega_o' = \gamma(B_o + Gx), \quad \text{Eq. 3}$$

and where γ is the gyro magnetic ratio. See e.g., FIG. 2.

Each spin then produces a voltage by magnetic induction in the receiver coil whose frequency spectrum consists of equally spaced sidebands $n\Omega$ centered at a Larmor frequency ω_o' corresponding to the location x of each spin. The amplitude of each sideband is given by:

$$J_n \left(\frac{\gamma b_0}{\Omega} \right) \quad \text{Eq. 4}$$

The instantaneous periodic angular velocity:

$$\omega' = \gamma b \quad \text{Eq. 5}$$

$$\text{where } b_0 = \mu h_0 \quad \text{Eq. 6}$$

of each spin is in phase with the time-varying component of its ambient magnetic field b_0 which is a function of the current flux distribution J . If the current distribution is uniform, the instantaneous angular velocity of each spin will be in phase with, and the angular phase of each spin will be displaced from, the applied electric field and from the applied voltage V by the loss angle δ as would occur in a uniform sample in the measurement application. If there are focal aberrations in complex permittivity, complex conductivity, and/or electrical impedance as are associated with spatially distributed foci of breast pathology, then there will be local aberrations in the magnetic field phase and intensity, focally distorting the image produced by the conventional magnetic resonance imaging machine identifying the spatial location of pathology for further evaluation or for treatment. Analysis of the signal

from these regions of distortion will produce an estimate of the complex permittivity, complex conductivity, and/or electrical impedance of the aberration which would help identify the nature of the pathology. The detector circuit **130** (see FIG. 6) according to an embodiment of the invention can measure the complex permittivity, complex conductivity, and/or electrical impedance at the phase modulating frequency Ω .

FIG. 3 represents the band spectrum of a frequency group produced by a clinical magnetic resonance imaging machine during the "read" time (as is known in the art). As shown in FIGS. 4A and 4B, the superposition of FIG. 3 and FIG. 2 produce a local aberration of signal distribution.

FIG. 5 represents the phase relationship of the voltage \check{V} of frequency Ω applied to the Faraday shield device, the electric field \check{E} thereby created, the local complex admittance \check{Y} or impedance \check{Z} , the local current flux density \check{J} , the temporal orthogonal components \check{J}_r and \check{J}_i of \check{J} , the orthogonal components \check{H}_r and \check{H}_i of the magnetic field intensity \check{H} produced by \check{J} , and the electric loss angle δ of the complex conductivity. Note that \check{E} corresponds to a spatial vector and \check{E} corresponds to a spatial and temporal vector.

FIG. 6 shows an exemplary detector/circuit for the demodulation of the Larmor frequency and, according to this embodiment of the present invention, for the detection of the temporal orthogonal components of each sideband of the line spectrum resolved with respect to the phase of the voltage \check{V} applied to the Faraday shield device, which yields $\tan \delta$, wherein δ is the electric loss angle. The detector provides cross-correlation with the voltage \check{V} applied to the Faraday shield for each side band. This cross correlation permits the detection of weak signals in the presence of noise. The received signal can thus be resolved as two components, one component in phase and one component 90 degrees out of phase, with the applied voltage \check{V} .

The detector of FIG. 6 can be utilized as an attachment to all magnetic resonance imaging devices for the determination of the complex permittivity, complex conductivity, and/or electrical impedance at a point x corresponding to frequency ω_0 . For example, as shown in FIG. 8A, a first image is of a breast with the Faraday shield voltage turned off. The second image, FIG. 8B, is an image of the same breast with the Faraday shield voltage turned on. Post processing can thus be used to measure, e.g., the complex permittivity at points of interest **200**, which can be representative of local aberrations. The results at each location can be compared to values stored in look-up tables or the like as a function of frequency. Further data reduction is also contemplated, as would be apparent to one of ordinary skill in the art given the present description.

The detector of FIG. 6 can be utilized as an attachment to magnetic resonance devices for continuous homogeneous sample analysis, where δ corresponds to the electric loss angle of the sample.

The detection circuit **130** shown in FIG. 6 is shown in analogue form. As would be apparent to one of ordinary skill in the art given the present description, circuit **130** can be designed as a digital circuit. Thus, circuit **130** of FIG. 6 can be implemented as a sideband detector. The ratio of the resolved real and imaginary components of the sidebands is tangent δ , determining the electric loss angle. As is known, complex permittivity is a point function, the real component of which corresponds to the complex conductivity. When implemented in a magnetic resonance measurement device for homogeneous sample analysis, the output of circuit **130** can be calibrated to measure the total electrical impedance.

In FIG. 6, a circuit **130** according to an embodiment of the present invention is coupled at amplifier **118** to a magnetic

resonance device (not fully shown for simplicity). As is known in the art, a local receiver coil **100** of the magnetic resonance machine is coupled to an impedance matching circuit **102**, feeding a noise matching preamplifier **104** through a protection circuit **106**. The output of the noise matching preamplifier is fed to an RF amplifier **108**, the output of which is directed to a double-balanced (synchronous) demodulator **110**, **112**. The output of the double-balanced demodulator **110**, **112** is fed through a summing amplifier **114** to an amplifier **116** and, according to this embodiment of the present invention, also to circuit **130** at amplifier **118**. Each of the demodulators **110** and **112** is supplied by a quadrature output at frequency ω_0' , which can be operator selected to correspond to a position x offset from the magnetic resonance master radio frequency oscillator. The demodulated outputs are then added at a summing amplifier **114** to provide input to the amplifier **116** which can feed to an imaging computer, as well as to amplifier **118** (which can be a low frequency amplifier) that, in turn, feeds additional sets of double-balanced demodulators **120**, **121**, each of whose cross-correlated outputs is the real or imaginary components of the signal received by the receiver coil from location x , corresponding to frequency ω_0' , resolved with respect to the phase of V , the voltage applied to the Faraday shield device. The ratio of each real and imaginary signal yields the electric loss tangent δ at location x , which defines the complex permittivity at frequency Ω . The output of the detector/circuit **130** can be directed to a computer or processor ("imaging computer") for digitization and/or for calculation/display of the complex permittivity values/integrated image in accordance with the description above. In addition, the computer or processor can be continually supplied with stored values at each location for further post measurement processing and data reduction.

According to alternative embodiments, the frequency Ω can be made continuously variable yielding the electric susceptibility as a function of the frequency.

According to an alternative embodiment of the present invention, the above methodology is also applicable to electron spin resonance magnetic resonance devices for measurements at extremely high frequencies.

The invention provides several advantages. The present method and system can be used for non-invasive breast cancer screening. For example, injection of Gadolinium compounds is not required, but may be performed for supplemental imaging, as is known in the art. Further, there is no ionizing radiation. Additionally, the frequency of measurement or mapping can be varied for further analysis. Further, the signal from fatty tissue need not be suppressed, as it must be in magnetic resonance mammography.

The foregoing description of the invention has been presented for purposes of illustration and description. It is not intended to be exhaustive or to limit the invention to the precise form disclosed, and modifications and variations are possible in light of the above teachings or may be acquired from practice of the invention. The drawings and description were chosen in order to explain the principles of the invention and its practical application. It is intended that the scope of the invention be defined by the claims and their equivalents.

I claim:

1. A method of detecting and evaluating sample spatially ordered pathology, comprising:

placing an in-vivo human tissue sample to be evaluated within a magnetic resonance imaging device in proximity to a Faraday shield device, wherein the Faraday shield device comprises Faraday shields oriented so as not to significantly affect a radio frequency field gener-

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ated within the magnetic resonance imaging device, and an insulating material that insulates the in-vivo human tissue sample from the Faraday shields, whereby the Faraday shield device is configured to apply a time varying potential difference to the in-vivo human tissue sample;

applying a time varying potential difference to the Faraday shield device, so as to create a time varying electric field in the in-vivo human tissue sample and a local time varying current field in the in-vivo human tissue sample essentially orthogonal to the main magnetic field generated by the magnetic resonance imaging device which results in a periodic aberration in a local magnetic field that periodically varies a phase of spins within the in-vivo human tissue sample; and

imaging at least one of a complex permittivity, a complex conductivity, and an electrical impedance of the in-vivo human tissue sample.

2. The method according to claim 1, wherein the in-vivo human tissue sample is a human breast, and wherein the Faraday shield device further comprises a pair of compression paddles containing the Faraday shields oriented in parallel to each other, wherein the compression paddles substantially align with a main magnetic field of the magnetic resonance imaging device.

3. The method according to claim 2, wherein the Faraday shields comprise electrically connected substantially parallel conducting elements oriented substantially orthogonal to the main magnetic field of the magnetic resonance imaging device.

4. The method according to claim 3, wherein the conducting elements of a Faraday shield are held at a common electrical potential.

5. The method according to claim 3, wherein the compression paddles are non-conductive, the insulating material has a high dielectric constant, and the conducting elements are coupled to a voltage source that applies the time varying potential difference across the conducting elements.

6. The method according to claim 5, wherein the insulating material comprises one or more ferroelectric materials.

7. The method according to claim 1, further comprising determining an electric loss angle of the in-vivo human tissue sample.

8. The method according to claim 1, wherein the in-vivo human tissue sample is a portion of a human breast.

9. The method according to claim 1, wherein the insulating material comprises one or more low conductivity materials.

10. A method of detecting and evaluating sample spatially ordered pathology, comprising:

placing a Faraday shield device within an imaging region of a magnetic resonance imaging device;

placing an in-vivo human tissue sample to be evaluated in proximity to the Faraday shield device, wherein the Faraday shield device comprises Faraday shields oriented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device, said Faraday shields being disposed within a pair of compression paddles and an insulating material that insulates the in-vivo human tissue sample from the Faraday shields, whereby the Faraday shield device is configured to apply a time varying potential difference to the in-vivo human tissue sample;

applying a time varying potential difference to the Faraday shield device, so as to create a time varying electric field in the in-vivo human tissue sample and a local time varying current field in the in-vivo human tissue sample essentially orthogonal to the main magnetic field gener-

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ated by the magnetic resonance imaging device which results in a periodic aberration in a local magnetic field that periodically varies a phase of spins within the in-vivo human tissue sample;

placing at least one of a receiver coil or a transmitter-receiver coil of the magnetic resonance imaging device on or near a surface of the compression paddles;

analyzing an image of the in-vivo human tissue sample produced by the magnetic resonance imaging device to detect at least one of a complex permittivity, a complex conductivity, and an electrical impedance of the in-vivo human tissue sample; and

identifying focal aberrations contained only in an image produced by the magnetic resonance imaging device so as to locate pathology.

11. The method according to claim 10, further comprising detecting orthogonal components of each sideband of a line spectrum resolved with respect to the phase of an applied voltage.

12. The method according to claim 11, further comprising determining a ratio of the resolved real and imaginary components of the sidebands.

13. The method according to claim 10, further comprising detecting orthogonal components of each sideband of a line spectrum resolved with respect to the phase of a voltage applied at a frequency (Ω) much less than the Larmor frequency of the magnetic resonance imaging device (ω_0).

14. The method according to claim 10, further comprising detecting orthogonal components of each sideband of a line spectrum resolved with respect to the phase of an applied voltage at variable frequencies (Ω) much less than the Larmor frequency of the magnetic resonance imaging device (ω_0).

15. A method of imaging electrical impedance by the application of time-varying electric fields in an in-vivo human tissue sample, comprising:

placing the in-vivo human tissue sample in a magnetic resonance imaging device;

providing a detector to the magnetic resonance imaging device;

providing a Faraday shield attachment in proximity to the in-vivo human tissue sample, wherein the Faraday shield attachment comprises Faraday shields oriented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device that include electrically connected parallel conducting elements and an insulating material that insulates the in-vivo human tissue sample from the Faraday shields, whereby the Faraday shield attachment is configured to apply a time varying potential difference to the in-vivo human tissue sample;

applying a periodic potential difference across the in-vivo human tissue sample so as to create a time varying electric field in the in-vivo human tissue sample and a local time varying current field in the in-vivo human tissue sample essentially orthogonal to the main magnetic field generated by the magnetic resonance imaging device which results in a periodic aberration in a local magnetic field that periodically varies a phase of spins within the in-vivo human tissue sample; and

analyzing an image of the in-vivo human tissue sample produced by the magnetic resonance imaging device to detect an impedance of the in-vivo human tissue sample with the detector.

16. The method of claim 15, wherein the periodic potential difference across the in-vivo human tissue sample is a variable frequency (Ω) much less than the Larmor frequency of

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the magnetic resonance imaging device (ω_0), so as to measure the electrical impedance of the in-vivo human tissue sample at variable frequencies.

17. The method according to claim 15, wherein the in-vivo human tissue sample is a portion of a human breast.

18. A system for detecting and evaluating sample pathology, comprising:

a magnetic resonance imaging device configured to produce an image of an in-vivo human tissue sample, the magnetic resonance imaging device generating a main magnetic field and including at least one of a receiving coil or a transmitter-receiver coil;

a Faraday shield device comprising Faraday shields that include an insulating material that insulates the in-vivo human tissue sample from the Faraday shields oriented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device, and electrically connected, substantially parallel conducting elements oriented substantially orthogonal to the main magnetic field of the magnetic resonance imaging device, whereby the Faraday shield device is configured to produce a time varying electric field in the in-vivo human tissue sample;

a voltage source coupled to the conducting elements and configured to generate a periodic voltage at a frequency (Ω) creating a current in the in-vivo human tissue sample essentially orthogonal to the main magnetic field of the magnetic resonance device; and

a detector configured to analyze an image of the in-vivo human tissue sample produced by the magnetic resonance imaging device to detect one of a complex permittivity, a complex conductivity, and an electrical impedance of the in-vivo human tissue sample.

19. The system according to claim 18, wherein the detector comprises:

first demodulators supplied with a quadrature output at a Larmor frequency from a magnetic resonance master radio frequency oscillator;

a first amplifier configured to sum first output signals from the first demodulators;

a second amplifier configured to receive a second output signal from the first amplifier; and

second demodulators coupled to the second amplifier configured to provide cross-correlated outputs corresponding to at least one of real and imaginary components that correspond to a signal received by the at least one of a receiver coil or a transmitter-receiver coil from a location in the in-vivo human tissue sample, and corresponding to the frequency resolved with respect to a phase of a periodic voltage.

20. The system according to claim 19, wherein the second demodulators comprise a series of double-balanced demodulator pairs, each double balanced demodulator pair coupled to the second amplifier, configured to provide cross-correlated outputs corresponding to at least one of real and imaginary components of the signal received by the at least one of a receiver coil or a transmitter-receiver coil from the location in the in-vivo human tissue sample.

21. The system according to claim 19, wherein the second demodulators are supplied with frequency sources $\sin(n\Omega t)$ and $\cos(n\Omega t)$, wherein $n\Omega$ is the frequency of the periodic voltage and an integral harmonic frequency n of Ω , and t is a time quantity.

22. The system according to claim 19, further comprising a processor configured to analyze the cross-correlated outputs of the second demodulators and to provide the complex permittivity at the location at a frequency (Ω).

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23. The system according to claim 18, wherein the Faraday shield device comprises a pair of low-conductivity compression paddles containing the Faraday shields.

24. The system according to claim 23, wherein the at least one of a receiving coil or a transmitter-receiver coil is disposed on or near at least one of the compression paddles.

25. The system according to claim 18, wherein the periodic voltage is continuously applied.

26. The system according to claim 18, wherein the voltage source is pulsed.

27. The system according to claim 18, wherein the voltage source is timed to the event sequence of the magnetic resonance imaging device.

28. The system according to claim 18, wherein the in-vivo human tissue sample is a portion of a human breast.

29. A system for imaging the electrical impedance of an in-vivo human tissue sample, comprising:

a magnetic resonance imaging device;

a Faraday shield attachment adapted to be placed within the magnetic resonance imaging device and disposed in proximity to the in-vivo human tissue sample, wherein the Faraday shield attachment comprises Faraday shields, oriented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device, that include electrically connected conducting elements oriented substantially parallel to each other and substantially orthogonal to a main magnetic field of the magnetic resonance imaging device and an insulating material that insulates the in-vivo human tissue sample from the Faraday shields, whereby the Faraday shield attachment is configured to apply a time varying potential difference to the in-vivo human tissue sample;

a voltage source coupled to the conducting elements of the Faraday shield attachment and configured to apply a periodic potential difference across the in-vivo human tissue sample so as to create a time varying electric field in the in-vivo human tissue sample and a local time varying current field in the in-vivo human tissue sample essentially orthogonal to the main magnetic field of the magnetic resonance imaging device which results in a periodic aberration in a local magnetic field that periodically varies a phase of spins within the in-vivo human tissue sample; and

a detector coupled to the magnetic resonance imaging device to analyze an image of the in-vivo human tissue sample produced by the magnetic resonance imaging device to detect a value corresponding to an electrical impedance of the in-vivo human tissue sample.

30. The system according to claim 29, wherein the in-vivo human tissue sample is a portion of a human breast.

31. A method of detecting and evaluating sample spatially ordered pathology, comprising:

placing an in-vivo tissue sample that is a human breast to be evaluated within a magnetic resonance imaging device and into a Faraday shield device, wherein the Faraday shield device comprises Faraday shields oriented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device and an insulating material that insulates the breast from the Faraday shields, whereby the Faraday shield device is configured to apply a time varying potential difference to the breast;

applying to the Faraday shield device a time varying potential difference having a phase modulating frequency, so as to create a time varying electric field in the breast and a time varying current field in the breast essentially

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orthogonal to the main magnetic field of the magnetic resonance imaging device that periodically varies a phase of spins within the breast; and
 imaging the distribution of at least one of a complex permittivity and an electrical impedance of the breast at the phase modulating frequency. 5

32. The method according to claim 31, comprising measuring the distribution of the complex permittivity of the breast at the phase modulating frequency.

33. The method according to claim 32, comprising measuring the distribution of the complex permittivity at a phase modulating frequency of the time varying potential difference. 10

34. A system for detecting and evaluating sample spatially ordered pathology, comprising: 15

a magnetic resonance imaging device;
 means for applying a time varying potential difference to a Faraday shield device disposed in proximity to an in-vivo human tissue sample, so as to create a time varying electric field in the in-vivo human tissue sample and a local time varying current field in the in-vivo human tissue sample essentially orthogonal to a main magnetic field generated by the magnetic resonance imaging device which results in a periodic aberration in a local magnetic field that periodically varies a phase of spins within the in-vivo human tissue sample, wherein the Faraday shield device comprises Faraday shields oriented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device and an insulating material that insulates the in-vivo human tissue sample from the Faraday shields, whereby the Faraday shield device is configured to apply a time varying potential difference to the in-vivo human tissue sample; and 20 30

means for imaging at least one of a complex permittivity, a complex conductivity, and an electrical impedance of the in-vivo human tissue sample. 35

35. A system for imaging electrical impedance by the application of time-varying electric fields in an in-vivo human tissue sample, comprising: 40

a magnetic resonance imaging device comprising a detector;
 a Faraday shield attachment adapted to be disposed in proximity to the in-vivo human tissue sample within the magnetic resonance imaging device, wherein the Faraday shield attachment comprises Faraday shields, ori- 45

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ented so as not to significantly affect a radio frequency field generated within the magnetic resonance imaging device, that include electrically connected conducting elements substantially parallel to each other and an insulating material that insulates the in-vivo human tissue sample from the Faraday shields, whereby the Faraday shield attachment is configured to apply a time varying potential difference to the in-vivo human tissue sample; means for applying a periodic potential difference to the Faraday shield attachment across the in-vivo human tissue sample so as to create a time varying electric field in the in-vivo human tissue sample and a local time varying current field in the in-vivo human tissue sample essentially orthogonal to a main magnetic field generated by the magnetic resonance imaging device which results in a periodic aberration in a local magnetic field that periodically varies a phase of spins within the in-vivo human tissue sample; and

means for analyzing an image of the in-vivo human tissue sample produced by the magnetic resonance imaging device to detect an electrical impedance of the in-vivo human tissue sample with the detector.

36. A system for detecting and evaluating sample spatially ordered pathology in an in-vivo breast tissue, comprising:

a magnetic resonance imaging device;
 a Faraday shield device in proximity to the breast tissue, the Faraday shield device comprising Faraday shields oriented so as not to interfere with a radio frequency field generated within the magnetic resonance imaging device and an insulating material that insulates the breast tissue from the Faraday shields;

means for applying to the Faraday shield device a time varying potential difference having a phase modulating frequency, so as to create a time varying electric field in the breast tissue and a time varying current field in the breast tissue essentially orthogonal to a main magnetic field generated by the magnetic resonance imaging device that periodically varies a phase of spins within the breast tissue, whereby the Faraday shield device is configured to apply a time varying potential difference to the breast tissue; and

means for imaging the distribution of at least one of a complex permittivity and an electrical impedance of the breast at the phase modulating frequency.

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